


RESEARCH

Open Access



Synergistic effect of umbilical cord extracellular vesicles and rhBMP-2 to enhance the regeneration of a metaphyseal femoral defect in osteoporotic rats

Amelie Deluca^{1,2*} , Andrea Wagner^{1,3}, Patrick Heime^{3,4}, Christian Deininger^{1,5}, Florian Wichlas⁵, Heinz Redl^{3,4}, Eva Rohde^{6,7}, Herbert Tempfer^{1,3}, Mario Gimona^{6,8} and Andreas Traweger^{1,3}

Abstract

Background The aim of this study was to evaluate potential synergistic effects of a single, local application of human umbilical cord MSC-derived sEVs in combination with a low dose of recombinant human rhBMP-2 to promote the regeneration of a metaphyseal femoral defect in an osteoporotic rat model.

Methods 6 weeks after induction of osteoporosis by bilateral ventral ovariectomy and administration of a special diet, a total of 64 rats underwent a distal femoral metaphyseal osteotomy using a manual Gigli wire saw. Defects were stabilized with an adapted Y-shaped mini-locking plate and were subsequently treated with alginate only, or alginate loaded with hUC-MSC-sEVs (2×10^9), rhBMP-2 (1.5 μg), or a combination of sEVs and rhBMP-2 ($n = 16$ for each group). 6 weeks post-surgery, femora were evaluated by μCT , descriptive histology, and biomechanical testing.

Results Native radiographs and μCT analysis confirmed superior bony union with callus formation after treatment with hUC-MSC-sEVs in combination with a low dose of rhBMP-2. This finding was further substantiated by histology, showing robust defect consolidation 6 weeks after treatment. Torsion testing of the explanted femora revealed increased stiffness after application of both, rhBMP-2 alone, or in combination with sEVs, whereas torque was only significantly increased after treatment with rhBMP-2 together with sEVs.

Conclusion The present study demonstrates that the co-application of hUC-MSC-sEVs can improve the efficacy of rhBMP-2 to promote the regeneration of osteoporotic bone defects.

Keywords BMP-2, Extracellular vesicles, Exosomes, Drug delivery; osteoporosis, Metaphyseal defect

*Correspondence:

Amelie Deluca
amelie.deluca@stud.pmu.ac.at

¹Institute of Tendon and Bone Regeneration, Salzburg 5020, Austria

²Department of Traumatology, KABEG—Klinikum Klagenfurt am Woerthersee, Klagenfurt 9020, Austria

³Austrian Cluster for Tissue Regeneration, Vienna 1200, Austria

⁴Ludwig Boltzmann Institute for Traumatology, The Research Centre in Cooperation with AUVA, Vienna 1200, Austria

⁵Department of Orthopedics and Traumatology, Salzburg University Hospital, Paracelsus Medical University, Salzburg 5020, Austria

⁶GMP Unit, Spinal Cord Injury and Tissue Regeneration Centre Salzburg, Paracelsus Medical University, Salzburg, Austria

⁷Department of Transfusion Medicine, Salzburger Landeskliniken GesmbH, Paracelsus Medical University, Salzburg, Austria

⁸Research Program "Nanovesicular Therapies", Paracelsus Medical University, Salzburg, Austria



© The Author(s) 2024. **Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>. The Creative Commons Public Domain Dedication waiver (<http://creativecommons.org/publicdomain/zero/1.0/>) applies to the data made available in this article, unless otherwise stated in a credit line to the data.

Introduction

The prevalence of osteoporosis (OP), especially in postmenopausal women is steadily increasing and already affects more than 20 million individuals in the USA alone [1]. It is characterized by low bone mineral density (BMD), the deterioration of bone architecture which results in reduced bone strength and hence, increased susceptibility to fractures [2, 3]. The poor healing of such fractures is associated with a significantly increased patient morbidity and mortality [4].

Generally, failure of fractures to heal adequately leads to complications that are especially present in the elderly, such as pain, weakness, reduced mobility and deterioration of the overall health status [5]. Therefore, the development of novel effective therapies to improve osteoporotic fracture repair is in dire need. Next to bone grafting and highly sophisticated biomimetic scaffolds, platelet-rich plasma (PRP), various growth factors, and multipotent mesenchymal stromal cells (MSCs) have been utilized in preclinical and clinical studies to enhance bone repair [6, 7]. Although the application of MSCs has clearly been shown to improve bone repair [8], the benefits of autologous cell therapies are significantly reduced in the elderly [9], the largest target group for osteoporotic fracture treatment.

More recently, MSC-derived trophic factors, including secreted vesicles, are considered to mainly contribute to the efficacy of cell therapies. Small extracellular vesicles (sEVs) are nano-sized lipid-bound vesicles released from cells into the extracellular space [10]. Initial evidence that sEVs exert a therapeutic effect was provided by Bruno S. et al., who demonstrated that human bone marrow-derived MSC-sEVs were as effective as their parental cells in promoting kidney regeneration in a murine acute kidney injury model [11]. Since then, a number of preclinical studies have demonstrated the potential of MSC-derived sEVs to promote musculoskeletal tissue repair [12], making them a promising contender for the treatment of bone disorders [13]. Interestingly, the co-administration of sEVs has also been demonstrated to amplify the efficacy of anti-cancer drugs *in vitro* [12] and to effectively reduce experimentally induced intrauterine adhesions *in vivo* when delivered together with estrogen [14]. Therefore, sEVs might also have the potential to enhance the efficacy of established bone repair therapeutics, including the administration of growth factors such as recombinant BMP-2.

Bone morphogenetic protein-2 (BMP-2), a member of the TGF- β superfamily, is a potent osteoinductive cytokine and promotes MSC proliferation and differentiation [15]. Several clinical studies have been conducted to assess the safety and efficacy of recombinant BMP-containing devices for treatment of diaphyseal bone fractures, delayed union, tibial nonunion and spinal fusion

[16]. However, as supraphysiological doses have mostly been applied, local and systemic adverse events were reported, yielding an undesired clinical outcome. Therefore, strategies to lower the required dose of BMP-2 without a concurrent loss in efficacy are under investigation and of great interest.

The combination of osteoinductive scaffolds with umbilical cord-derived mesenchymal stem cell-secreted extracellular vesicles (UC-MSC-sEVs) has previously shown promising results in enhancing *in vivo* bone repair [17, 18]. While this approach has demonstrated efficacy, there is an intriguing potential for the combination of human hUC-MSC-sEVs with a low dose of recombinant human (rh)BMP-2 to further enhance bone healing. This strategy not only could improve the therapeutic outcome, but also has potential to mitigate any safety concerns associated with the use of higher doses of rhBMP-2. Hence, the primary objective of the current investigation was to explore the possible effects of hUC-MSC-sEVs in amplifying rhBMP-2-mediated bone repair, particularly in the context of osteoporotic bone, employing a metaphyseal defect model in rat femurs.

Materials and methods

Experimental animals

All animal experiments and conducted procedures were in accordance with the law on animal experimentation and are approved by the regulatory authorities. The work has been reported in line with the ARRIVE guidelines 2.0.

A total of sixty-four 12-week-old, adult female Sprague Dawley rats (Janvier Labs SAS, France) weighing approximately 300–350 g were randomly assigned to either one of four experimental groups of equal size ($n=16$; see 2.2 for details). The animals were kept under standard housing conditions (2–3 rats per cage) with free access to food and water. Post-operatively the same animals were kept in groups of 2 to 3 rats per cage. Rooms were maintained at 25 ± 2 °C and a 12:12 h light/dark cycle, light on at 07:00 h.

Animal study design and surgical procedures

After an appropriate acclimatization phase, all rats underwent a ventral ovariectomy (OVX, $n=64$) and osteoporosis was further induced by feeding a calcium-, phosphorus-, vitamin D3-, soy- and phytoestrogen-free diet (Altromin-C1034, Altromin Spezialfutter GmbH, Lage, Germany) for a total of six weeks as previously described in Deluca et al. [17]. Subsequently, all animals underwent right femoral surgery to create an osteotomy gap with a Gigli wire saw as published [17]. Briefly, thirty minutes preoperatively all rats received 0,03 mg/kg buprenorphine as a subcutaneous (s. c.) injection and inhalation anesthesia (isoflurane) was induced. Body

temperature was maintained using a heating pad (Harvard Apparatus, Holliston, MA, USA) and prior to surgery, each animal received an antibiotic (Clindamycin s.c., 45 mg/kg). After aseptic preparation, the femur was exposed from the lateral femoral condyle to the lateral midshaft area. The capsule of the knee joint was opened, and the patella dislocated medially. Prior to performing the osteotomy, the femur was stabilized using an adapted Y-shaped interlocking plate (Veterinary Orthopedic Implants Inc., 1.5 mm Condylar Angle Stable, DT Locking 2×6 hole; Orly, France). Subsequently, a distal metaphyseal osteotomy was set with a 0.66 mm Gigli wire saw (RISystem AG, Lanquart, Switzerland). The site was thoroughly rinsed with sterile saline solution. Defects were then treated according to the following groups (see also Fig. 1): Alginate hydrogel only (AH), AH+hUC-MSC-sEVs (sEVs; dose: 2×10^9), AH+rhBMP-2 (dose 1.5 µg; Peprotech, Vienna, Austria), AH+rhBMP-2+sEVs (2×10^9 and 1.5 µg respectively). The final volume of the implanted alginate clot was 80 µl using alginate at a final concentration of 1.5 mg/ml (PRONOVA SLG-20; NovaMatrix, Sandvika, Norway). Wound closure was performed in layers with closure of the joint capsule, muscle sutures and sterile surgical clips (FST, Heidelberg,

Germany). Immediately post-operatively, a control X-ray was performed to confirm the accurate placement of the osteosynthesis. As postoperative analgesia the animals received a daily dose of buprenorphine (0.03 mg/kg, twice daily) for a total of 72 h and oral tramadol-hydrochloride (20 mg/kg body weight, once daily) via their drinking water for a total of 7 days. The animals had free access to food and water and were frequently monitored for any complications, weight loss or abnormal behavior.

Four- and six-weeks post-treatment rats were euthanized were euthanized by intracardial barbiturate injection (Pentobarbital-Natrium 300 mg/mL; Release, WDT, Germany) under general isoflurane anesthesia and the femurs were harvested and prepared for subsequent µCT, biomechanical, and histological analysis.

Preparation of hUC-MSC-sEVs

Umbilical cord material was gathered following the uncomplicated delivery of healthy newborns from women who had previously provided written informed consent during an earlier stage of pregnancy (Department of Obstetrics and Gynecology; University Clinic Salzburg). The approval to use human umbilical cord MSCs was obtained from the Ethics Committee of the

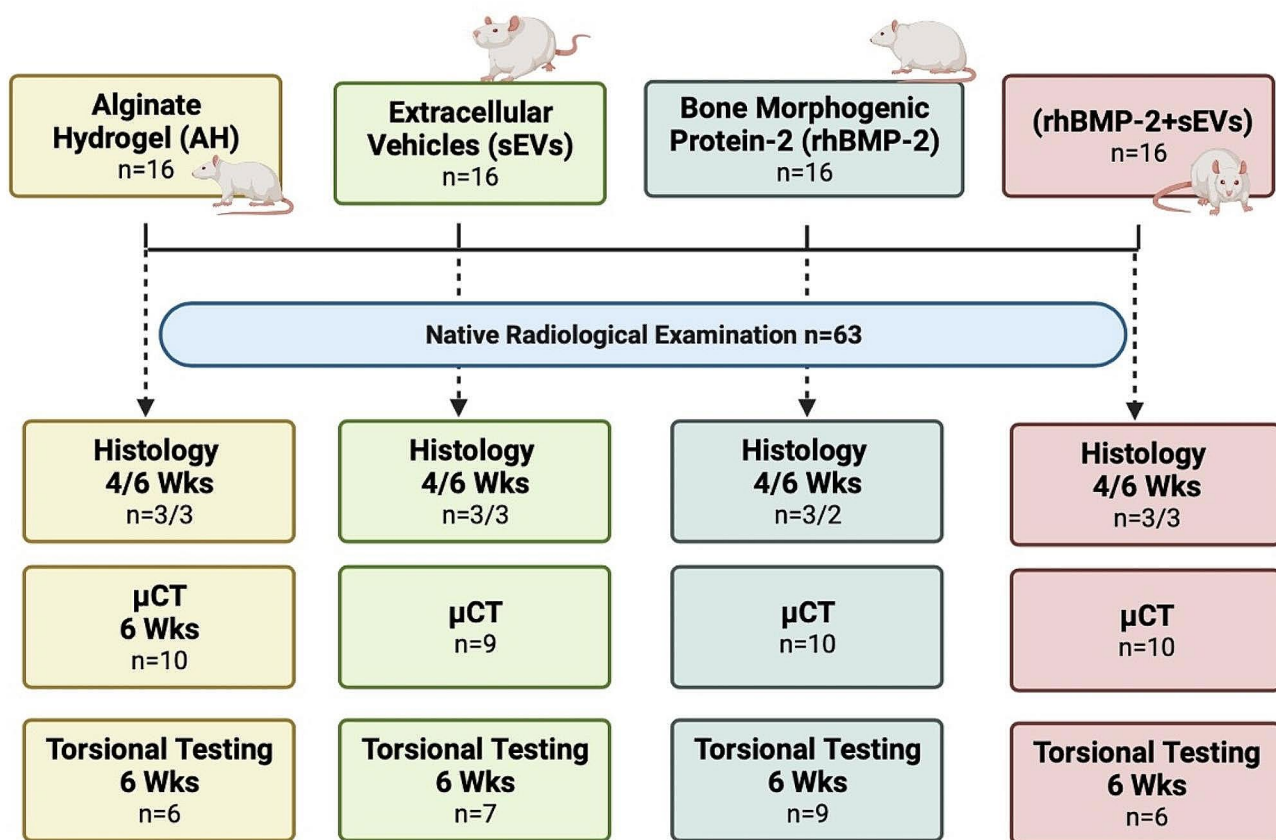


Fig. 1 Overview of groups according to the applied biomaterials and used follow-up procedures including native radiographs, histology, micro computed tomography (µCT), analysis, and torsional testing. Wks = weeks

province of Salzburg (protocol 415-E/1776/4-2014). Following delivery, cords were promptly collected and preserved in phosphate-buffered saline (PBS) for subsequent processing as previously described [18]. The entire cords were washed in PBS to remove contaminating blood cells, after which the cord stroma was cut into 1–2 mm³ fragments. These pieces were then placed in a culture plate, allowing them to adhere before adding culture medium - α -MEM (Sigma-Aldrich) supplemented with 10% (v/v) pooled human platelet lysate (pHPL) and Dipeptiven (5.5 mg/mL, Fresenius-Kabi, Graz, Austria). After 10–12 days, visible UC-MSC colonies had formed and the remaining cord tissue fragments were removed. UC-derived MSCs were enzymatically detached using TrypLE Select CTS (A12859-01, Gibco) and subsequently expanded in cell factory systems (CF4, Thermo Scientific). Immunophenotype and viability analysis of MSCs were conducted following the marker profile suggested by the International Society of Cell Therapy (ISCT) in 2005. hUC-MSCs were expanded from cryopreserved stocks in a fibrinogen-depleted culture medium (α -MEM supplemented with 10% v/v pooled human platelet lysate and 5.5 mg/mL dipeptiven; Merck, Vienna, Austria) and subsequently, upon reaching 60–70% confluency the growth medium was exchanged with vesicle-depleted harvest medium (α -MEM supplemented with 5% v/v pooled human platelet lysate, 5.5 mg/mL dipeptiven). Cells were cultured for a total of 24 h and culture supernatants were collected, centrifuged at 2.500 \times g for 20 min to pellet cell debris and the supernatants were then sterile filtered (0.22 μ m; Merck, Vienna, Austria). Processed culture media were concentrated by tangential flow filtration (TFF) (100 kDa hollow fiber filter, Spectrum Labs-Repligen, Breda, The Netherlands) and buffer-exchanged into sterile PBS by diafiltration. Finally, hUC-MSC-sEVs were collected by ultracentrifugation (120 000 \times g, 3 h at 18 °C). hUC-MSC-sEVs were resuspended in sterile Ringer's lactate at a final concentration of 2 \times 10⁹ particles per 15 μ l. Particle size and amount were determined using a nanoparticle tracking (NTA) device in light scatter mode (ZetaViewPMX 110, Particle Metrix; Inning am Ammersee, Germany) and total protein content was determined by fluorescence spectroscopy (Qubit 3.0; Life Technologies; Vienna Austria). Finally, sEV surface protein profiling was conducted using the MACSPlex Exosome Kit according to the manufacturer's instructions (Miltenyi Biotec; Bergisch Gladbach, Germany).

Histological examination and staining

Four- and six-weeks post-treatment three animals ($n=3$) of each group were euthanized and the right femur, including muscle tissue, was explanted by exarticulation at the knee and hip joint and were then fixed in 4% paraformaldehyde (PFA) in PBS at 4–6 °C. For the

AH+rhBMP-2 group one animal died after surgery (see [results](#) section) and therefore for the time point 6 weeks after surgery only 2 samples were available. After 48 h, samples were decalcified in 2% PFA/ 12.5% EDTA solution (pH=7.5). After a minimum of 7 weeks the femora were evaluated by X-ray to ensure complete decalcification. After removing the screws and osteosynthesis plate, samples were then processed for paraffin embedding. 6 μ m sections were prepared and deparaffinized using Roti[®]-Histol (Carl Roth, Germany), rehydrated in a graded alcohol series and stained with Masson-Goldner trichrome stain or Alcian blue/Nuclear Fast Red Acid [19] according to standard procedures. Digital high-resolution images were acquired on an Olympus VS120 slide scanner (Olympus, Vienna, Austria).

Radiological evaluation and μ CT analysis

Healing was monitored by two independent observers. Anteroposterior and lateral radiological views were acquired under general anesthesia immediately post-operatively, after 1 and 2 weeks and then at biweekly intervals for all animals.

After fixation in 4% PFA in PBS, osteosynthesis plates were carefully removed, ensuring no fracture occurred. One sample of the AH-sEV group was excluded, as the femur broke during preparation (see [Fig. 1](#)). During μ CT scanning, explanted femora were stored in polymer sample tubes filled with formalin to prevent dehydration. Of each group, nine to ten ($n=9-10$) samples were scanned in a SCANCO μ CT 50 (SCANCO Medical AG, Brüttsellen, Switzerland) at 70 kVp, 114 μ A filtered with 0.5 mm Al. Over a field of view of 20.4 mm, 850 Projections/180° were integrated for 475 ms with averaging 1, HW-binning 2 and reconstructed to an isotropic resolution of 12 μ m. Scans were exported as DICOM slices calibrated to mgHA/cm³. Image preprocessing and measurements were performed using Fiji [20] and Definiens Developer XD 2.7 (Definiens AG, Munich, Germany). Bone Volume (BV) over total Tissue Volume (TV) was determined for the defined, encompassing the newly formed bone in the medullary canal, within the osteotomy region, and the periosteal callus within a defined ROI (for further details see supplementary information). BV/TV are expressed in %.

Radiological and histological scoring

All native radiographs, μ CT images, and histological sections were evaluated by three independent observers (Author 1, 4, and 10) who were blinded to the groups. The radiographs and μ CTs were scored for callus formation, quality of union, and bone remodeling after 6 weeks as previously described [17, 21] and summarized in [Table 1](#). The maximum expected total score is 8 for bone fracture repair. The histological sections were evaluated

Table 1 Radiographic scoring system for fracture healing

Categories	Scores			
	3	2	1	0
Periosteal reaction	Complete across defect	Moderate (> 50%)	Mild (< 50%)	None
Bone union	Complete bony union	Moderate (> 50%)	Mild (< 50%)	None
Remodeling		Complete remodeled cortex	Mild (< 50%)	None

Table 2 Histological scoring system for fracture healing

Categories	Scores			
	3	2	1	0
Callus formation	Complete across defect	Moderate (> 50%)	Mild (< 50%)	None
Bone union	Complete bony union	Moderate (> 50%)	Mild (< 50%)	None
Cortex remodeling	Complete remodeled cortex	Moderate (> 50%)	Mild (< 50%)	None
Marrow changes	Adult type fatty marrow	Moderate (> 50%)	Mild (< 50%)	None

by the same investigators for fracture healing and scored as summarized in Table 2 [17, 21] at 4 and 6 weeks after treatment. The maximum total histological score for bone fracture healing achievable is 12.

Biomechanical analysis

After μ CT was performed, samples underwent torsion testing using an adapted universal tensile testing machine (Zwick / Roell; Ulm Germany). Therefore, the femora were proximally and distally embedded in resin (Ren-Cast[®] FC 53; Biesterfeld AG, Hamburg, Germany), ensuring the embedding was along the longitudinal axis of the diaphysis and without any contact to the defect area. Misaligned samples were excluded. After applying a preload of 0.2 N, samples were loaded at a constant speed of 0.1 mm/sec. The endpoint was set as a fracture of the femora which occurred in the pre-determined metaphyseal fracture zone. Samples fracturing at a different region were excluded from the analysis. Torque (Nmm) and torsional stiffness (Nmm/°) were determined from the torque vs. rotation curve. Tissue stiffness was determined from a linear region between a rotation angle of 0.5° and 1.5°.

Statistical analysis

All obtained data samples are reported as means \pm standard deviations. Datasets were tested for normal distribution using the Shapiro Wilk test. A one-way ANOVA test with post-hoc pairwise.

comparison (Tukey's) or for pairwise comparisons an unpaired t-test was used. Statistical significance was set at $P=0.05$. All tests were performed using GraphPad Prism v. 9.02 (La Jolla, CA, USA).

Results

Characterization of hUC-MSC-sEVs

Nanoparticle tracking analysis (NTA) revealed a mean sEV size of 139 nm and total protein content was 1050 μ g/mL. Bead-based multiplex analysis revealed the

robust expression of the sEV tetraspanins CD9, CD63, and CD81 in addition to CD29 (Integrin beta- 1), the MSC-EV-specific markers CD44 (hyaluronic acid receptor) and MSCP/NG2 (melanoma-associated chondroitin sulfate proteoglycan) (see Fig. 2).

General Animal health

In total, 63 out of 64 animals reached the endpoint of 6 weeks after the second surgery. One animal (rhBMP-2) died shortly after the metaphyseal defect surgery for unknown reasons. Overall, no severe intra-operative complications occurred and all animals showed normal behavior, with full weight bearing 24 h after surgery. No animals were excluded in the further course due to weight loss or other signs of postoperative complications.

Radiographic evaluation

The obtained X-rays immediately post-surgery, after 1 week, and followed by biweekly intervals were analyzed and documented for comparison (Fig. 3). Defects created with the 0.66 mm Gigli saw and treated with AH only demonstrated minimal bony bridging with minimal to no callus formation. Defects treated with AH+sEVs showed moderate bony bridging with minimal callus formation. Similarly, the application of AH with a low dose of rhBMP-2 also yielded bony bridging identical to the bridging observed in the femora treated with AH+sEVs. A persistent non-union was not observed for any of the samples. However, significant callus and bone formation was mainly observed 6 weeks after addition of alginate hydrogel loaded with a combination of a low dose of rhBMP-2 and hUC-MSC-derived (Fig. 3, bottom row).

Histology

4 weeks after treatment of the defects, for all samples only minor cortical bridging and callus formation were evident by descriptive histology. 6 weeks post-treatment, femora treated with AH samples presented upon histological staining with partially extensive callus formation

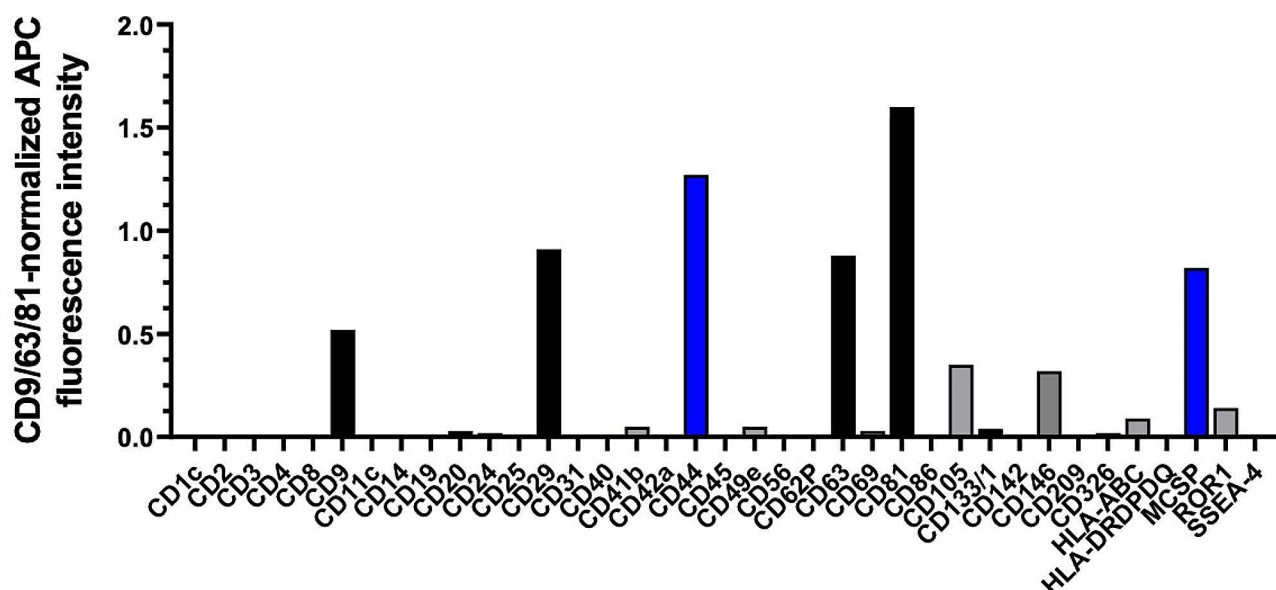


Fig. 2 MASCSplex profiling of hUC-MSC-sEV preparation. Bar graph shows the robust expression of the sEV marker proteins CD9, CD29, CD63, and CD81 (black bars). In addition, the MSC-EV-specific markers CD44 and MSCP/NG2 were clearly present (blue bars)

but little bony bridging. In contrast, the bony bridge after application of AH+sEVs was more enhanced with bony callus formation and active bone remodeling within the defect area. For AH+rhBMP-2-treated femora an increasing osseous continuity and less callus formation was seen in Masson Goldner Trichrome-stained (Fig. 4) and by Alcian blue-stained (see Suppl. Figure 1) FFPE sections. Sections from AH-rhBMP-2+sEVs-treated samples displayed complete remodeled cortices and minimal callus formation. Together, the histological examination was concurrent with the radiographic findings.

Microcomputed tomography

BV/TV was determined for the defect area, including the callus volume and the newly formed bony tissue within the medullary canal (see Suppl. Figure 2 for segmentation strategy). However, there were no significant differences evident when comparing the volumes of the newly formed bone tissue (Fig. 5A/B). Analysis of sagittal μ CT sections however confirmed the overall findings by descriptive histology and radiography. None of the samples of the AH group showed a full consolidation of the defect, only a mild periosteal reaction with initial bony remodeling and incipient callus formation. Samples in the AH+sEVs group showed fracture healing by mild to moderate callus formation. The fracture itself however exhibited no bony union with the cortices being largely open. Animals treated with rhBMP-2 also showed mild to moderate callus formation and only one out of ten samples revealed complete bony bridging. Analyzed sections from samples treated with rhBMP-2 in combination with hUC-MSC-sEVs presented with more extensive callus

formation, a moderate to complete periosteal reaction around the defect and moderate to complete bony union. Representative images are shown in Fig. 5A.

Radiological and histological scoring

To further determine the extent of bony union, all histological Sect. (6 weeks post surgery) and radiographic images (native radiographs and μ CT sections combined) were evaluated for bone repair as described in the methods section, further substantiating our findings by qualitative analysis (summarized in Table 3). Histological scoring for the AH group showed partially extensive callus formation, no union with mild cortex remodeling, and a mean total histological score of 5 ± 1 . Samples treated with AH-sEVs presented with moderate to extensive callus formation, moderate bony union, extensive remodeling of the cortices and the marrow with a mean score of 7 ± 1 . Femora after application of AH-rhBMP-2 to the defect showed widespread remodeling with callus formation, pronounced bony union at the fracture site (full union evident for 1 out of 10 samples) with cortex remodeling and abundant marrow changes with new bone formation; mean total score 9 ± 1 . Defects treated with AH-rhBMP-2+sEVs demonstrated mostly complete bony union, marrow remodeling to the consistency of regular healthy bone tissue, moderate callus formation with a mean total histological score of 11 ± 1 (summarized in Table 3).

Analyzing the radiological mean scores of samples in the AH group, resulted in a mean total score of 5 ± 1 with a complete periosteal reaction and mild bony union. Samples of the AH-sEVs and AH-rhBMP-2 group were

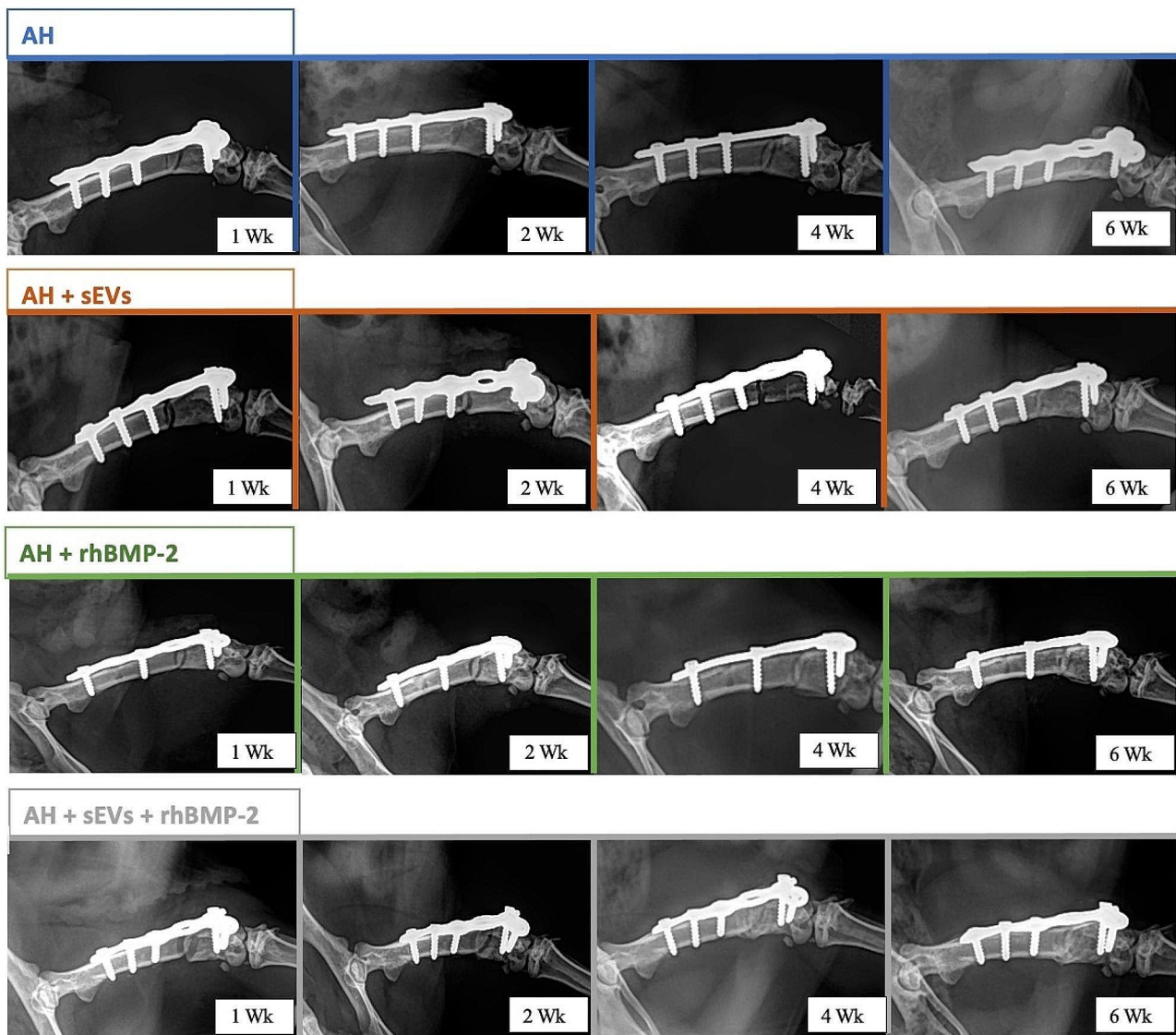


Fig. 3 : Radiological follow-up 1-, 2-, 4- and 6-weeks post-surgery after distal femoral plate fixation. The defect was treated with either alginate only (AH), alginate with huUC-MSC-sEVs (AH + sEVs), alginate with rhBMP-2 (AH + rhBMP-2) or alginate with a combination of BMP-2 + sEVs (AH + rhBMP-2 + sEVs)

classified with a radiological mean total score of 6 ± 1 . The analysis of the native radiographs demonstrated a complete periosteal reaction, moderate bony union and incipient remodeling with callus formation. Femurs treated with AH-rhBMP-2+sEVs yielded a mean total score of 8 ± 1 , with a complete periosteal reaction and new bone formation, broad fracture union, and remodeling with additional callus formation around the fracture site.

Biomechanical analysis

To evaluate functional defect healing, torsional testing was performed 6 weeks after treatment, determining torque (Nmm) and the torsional stiffness (Nmm/°). Numerous samples had to be excluded from the analysis. This exclusion was based on the observation of

creep, as indicated by the torque versus torsional angle function, or because the sample did not undergo fracture at the intended defect site. A significant difference in maximum torque was evident when comparing samples from the treatment groups AH and AH+rhBMP-2+sEVs ($*P=0.0280$), AH-sEVs and AH+rhBMP-2+sEVs ($**P=0.0028$), and AH+rhBMP-2 to AH+rhBMP-2+sEVs ($***P=0.0109$; Fig. 6A). Therefore, it can be concluded that the combination of rhBMP-2 and sEVs resulted in significantly more stable bony consolidation, which was closest to untreated, healthy femora. These results further substantiate the results from the histological and radiological evaluation. Surprisingly, the analysis of the torsional stiffness showed only significant difference when comparing the AH-sEVs

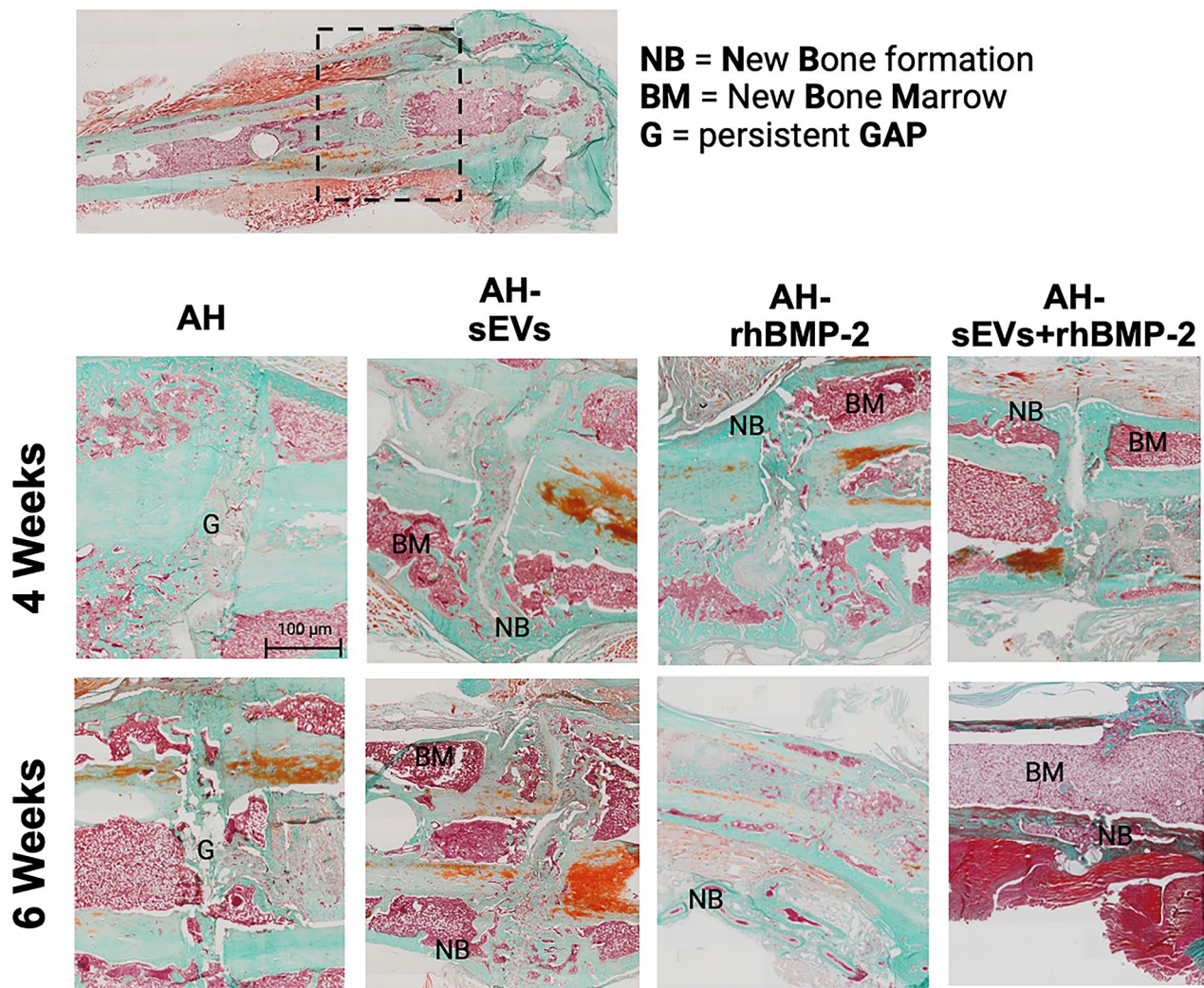


Fig. 4 : Histological evaluation 4 and 6 weeks after treatment of Masson Goldner trichrome-stained FFPE sections. Dashed lines indicate the defect area. Scale bar = 100 μm

and AH-rhBMP-2+EVs groups (**P*=0.0152; Fig. 6B). Interestingly, all femora that had either been treated with rhBMP-2 alone or sEVs in combination with rhBMP-2 revealed stiffness values comparable to the untreated femora.

Discussion

The objective of the current study was to explore the possible synergistic effects of human umbilical cord-derived mesenchymal stem cell-secreted extracellular vesicles in enhancing rhBMP-2-mediated bone repair in osteoporotic bone, utilizing a previously established metaphyseal rat femur defect model [17]. Based on the analysis of native X-rays, semi-quantitative and descriptive histology, micro-computed tomography (μCT), and biomechanical evaluations, we demonstrate that a single, orthotopic administration of hUC-MS-C-sEVs in

combination with a low dose of rhBMP-2 resulted in the most favorable outcomes for fracture healing.

Significant differences in bone healing were evident in vivo between the various treatment groups, with a superior performance of the rhBMP-2+sEVs hydrogels. Native radiographs demonstrated mostly complete bony union, with remodeled cortices and callus formation. The same results were also observed by histological staining, where the initial fracture was almost completely resolved due to complete remodeling of the cortices via secondary fracture healing. In comparison, mean radiological and histological scores for samples in the AH, sEV, and rhBMP-2 groups showed inferior results. Most importantly, the biomechanical evaluation supported the results of the radiological and histological analyses, as the highest stability (torque) was determined for the group treated with sEVs in combination with rhBMP-2.

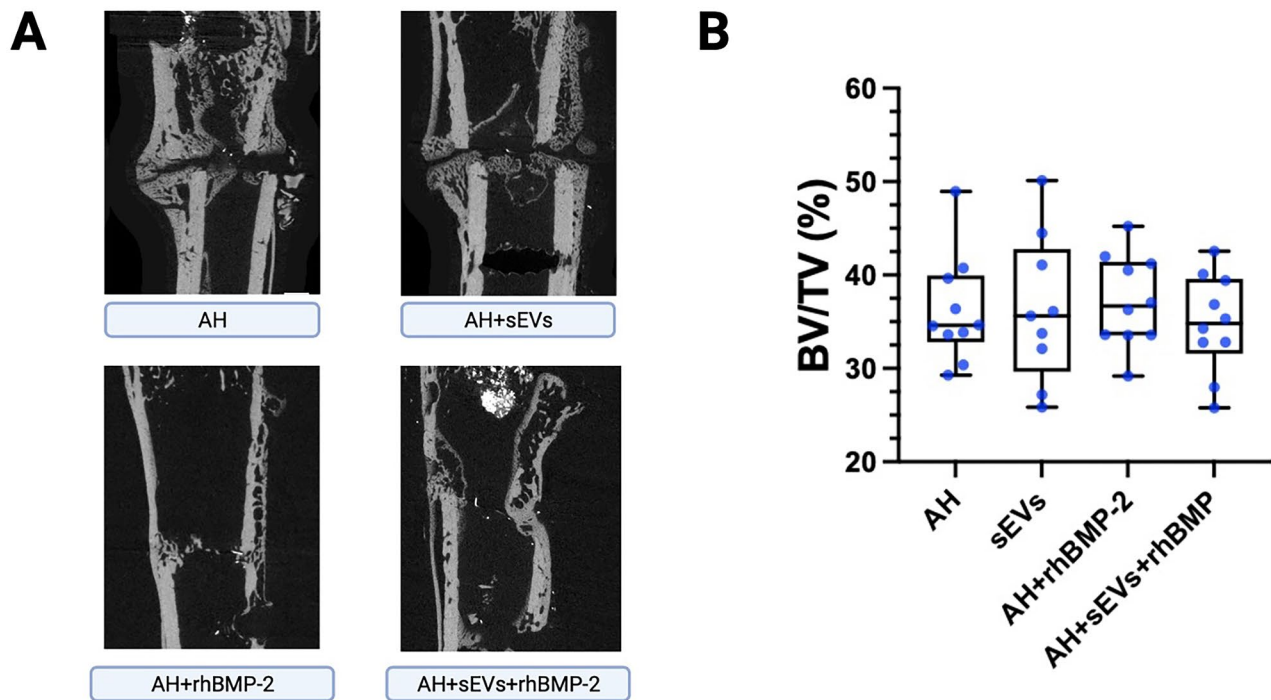


Fig. 5 μCT images of the defect area 6 weeks after treatment. **(A)** Representative sagittal μCT sections of the defect area. **(B)** Quantitative analysis of BV/TV for all 4 treatment groups, revealing no significant difference between the newly formed bone volume

Table 3 Summary of obtained histological and radiological mean scores

	AH	AH+sEVs	AH rhBMP-2	AH-rhBMP-2+sEVs
Histological mean score	5±1	7±1	9±1	11±1
Radiological mean score	5±1	6±1	6±1	8±1

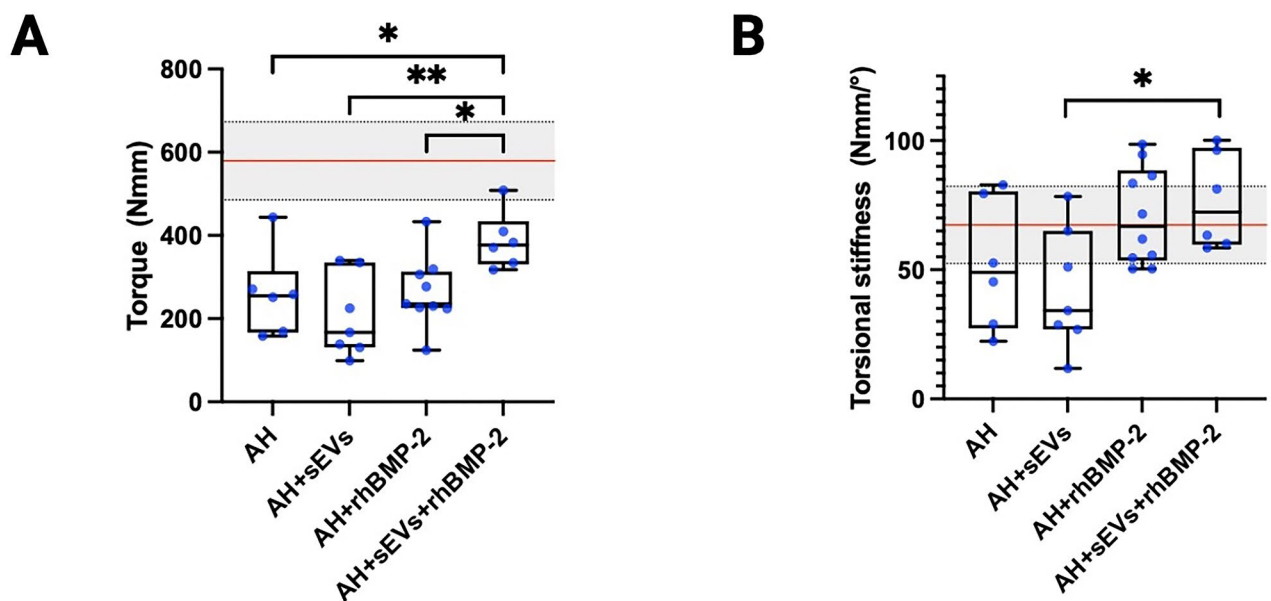


Fig. 6 Biomechanical analysis 6 weeks post-OP. **(A)** Torque and **(B)** torsional stiffness values determined for femora treated with alginate (AH), sEVs alone, rhBMP-2 alone, or rhBMP-2 in combination with sEVs. The red line indicates mean values determined for healthy femora, with ±1SD indicated (grey area). * = $p < 0.05$; ** = $p < 0.01$; *** = $p < 0.005$

The distal radius, proximal humerus, proximal femur, and vertebral bodies and their trabecular or metaphyseal bone regions are especially prone to osteoporotic fractures [22, 23]. As the aging population is expected to double by 2050 and the occurrence of osteoporotic fractures is to rise in the near future, impairment of osteoporotic fracture healing is an emerging public health concern [24]. Given that the animal model employed in this investigation assesses bone repair specifically in the femur metaphysis rather than the diaphyseal femur, our study more closely mirrors the clinical scenario, as the majority of osteoporotic fractures in long bones predominantly occur in the metaphyseal region. Other animal studies have already reported upon the enhanced fracture repair and stimulation of early new bone formation with rhBMP-2 in ovariectomized rats [21, 25]. But to our knowledge this is the first study to report on the effects of combining hUC-MSC-sEVs with a low dose of rhBMP-2 to promote osteoporotic bone healing.

The improved fracture repair, particularly evident in combination with rhBMP-2 rather than with standalone sEVs, strongly implies a primary role of sEVs as facilitators in delivering rhBMP-2 more efficiently to recipient cells. In addition to their function in internal cargo transport, it is now increasingly evident that sEVs strongly bind proteins on their surface, leading to the formation of a protein corona [26–28]. Various methods have been explored for loading therapeutic cargo to sEVs, including techniques such as sonication, electroporation, freeze-thawing, and co-incubation. Notably, passive loading of sEVs through co-incubation has demonstrated efficacy in delivering anti-VEGF antibodies, effectively reducing neoangiogenesis *in vivo* in a rat retinopathy model [29]. In this study, passive loading via simple co-incubation at room temperature was employed, chosen for its simplicity and minimal impact on sEV membrane integrity compared to various alternative methods.

sEVs have been demonstrated to convey immunomodulatory [30], anti-inflammatory, and anti-fibrotic activities [31, 32]. Therefore, it cannot be excluded that the observed enhanced effectiveness of rhBMP-2 for osteoporotic bone repair is also a consequence of pleiotropic actions of sEVs together with an enhanced delivery of rhBMP-2. Therefore, it is also possible that the observed enhanced efficacy of rhBMP-2 in osteoporotic bone repair is a result of the pleiotropic actions of sEVs in conjunction with an improved delivery of rhBMP-2. Nonetheless, the improved effectiveness of a low dosage of rhBMP-2, observed when co-applied with sEVs in this study, is likely attributed to a more effective delivery of the osteoinductive growth factor to the target cells. EV uptake and downstream bioactive effects may be dependent on membrane-bound protein interaction with the recipient cell [33–35].

The uptake of EVs and their downstream bioactive effects have been shown to depend on membrane-bound protein interactions with recipient cells [33, 35]. Among these proteins, several tetraspanins play a crucial role, with notable examples being CD9 and CD81. These have been demonstrated to possess fusogenic properties, implicating them in processes such as phagocyte fusion. A recent study by Xu J. et al. demonstrated the essential role of CD9 or CD81 in binding and subsequent bioactivity of extracellular vesicles derived from human perivascular stem cells on recipient osteoprogenitor cells [36]. The robust expression of CD9 and CD81 in the hUC-MSC-sEVs utilized in this study indicates an effective uptake of the extracellular vesicles, and consequently, of the co-administered rhBMP-2 by osteoprogenitor cells within the bone defect.

For optimal *in vivo* application, it is essential to consider the pharmacokinetics and distribution of exosomes. Typically, following intravenous injection, most extracellular vesicles (EVs) have been observed to distribute to the spleen, liver, lung, and kidney within 30 min, with an approximate half-life of 3 h in the blood [37]. In our study, the local delivery of hUC-MSC-sEVs, either alone or in combination with rhBMP-2, was intended to maximize concentrations at the defect site. This approach takes into account the generally brief half-life and swift cellular uptake kinetics of sEVs. Xu CM et al. demonstrated minimal MSC-EV uptake in other organs after local intramyocardial injection of EVs in a murine model of myocardial infarction [38]. Consequently, it is highly probable that the majority of the administered sEVs remained localized at the defect site. The precise determination of biodistribution following local administration would necessitate treatments with appropriately labeled sEVs. However, it is important to note that there have been reports highlighting challenges in obtaining accurate results when employing lipophilic fluorophore staining of extracellular vesicles for uptake studies [39, 40]. Addressing this concern would be pivotal for a comprehensive understanding of the fate of locally administered sEVs and is an avenue for further investigation to ensure the reliability and accuracy of the biodistribution assessments. The current study had additional limitations. Firstly, the animals were euthanized six weeks post-femoral surgery, thereby precluding the assessment of the long-term impact of the treatments on bone remodeling. Moreover, underlying cellular and molecular mechanisms potentially driving the observed synergistic effects, beyond a potentially improved growth factor delivery, require further investigations.

The results of our study are very promising and warrant a follow-up large animal study and potentially subsequent clinical evaluations. Among the available sources of MSCs, human umbilical cord is an economically viable,

productive, feasible, and universally applicable source. Numerous studies have documented the utilization of sEVs derived from hUC in the treatment of various diseases [41]. The translation of the approach outlined in this study is viable, given that rhBMP-2 (InFuse®) is clinically approved, and the small extracellular vesicles (sEVs) utilized in this study were prepared in accordance with Good Manufacturing Practice (GMP) standards. A comparable preparation has already been employed in a first-in-man study aimed at mitigating fibrotic adhesions following cochlear implant surgery [42]. So far, the usage of rhBMP-2 applied with a collagen scaffold has been approved by the U.S. Food and Drug Administration for the promotion of spinal fusion and fracture healing [43, 44]. However, some serious adverse events have been reported after the clinical application of rhBMP-2, mainly due to the use of excessive dosages resulting in ectopic bone formation and pronounced tissue inflammation [24, 45–47]. Considering that all reported major adverse events were associated with a supra-physiological dose, our findings that the co-application of naïve hUC-sEVs allows the reduction of an effective rhBMP-2 dose [48], bears great promise to improve the safety profile of BMP-2. Importantly, owing to their natural origin, small extracellular vesicles (sEVs) exhibit high biocompatibility and limited immunogenicity. These inherent characteristics confer potential advantages over conventional synthetic drug delivery vehicles, including liposomes and nanoparticles.

Conclusion

In summary, the simultaneous administration of rhBMP-2 and sEVs exhibited superior efficacy in healing osteoporotic defects compared to the individual administration of a low dose of rhBMP-2 or sEVs. Consequently, this approach holds the potential to reduce the dosage of rhBMP-2 required for treating osteoporotic fractures, thereby improving the safety profile associated with BMP-2 treatments.

Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s13287-024-03755-8>.

Supplementary Material 1

Acknowledgements

We thank Clemens Koller and his team for excellent animal care. Figures were in part created using Biorender.com. We further like to thank Bettina Faustini and Nadja Weissenbacher for the support for the establishment of the ovariectomy surgeries.

Author contributions

AD: study design, surgeries, histology, radiological analysis, figure preparation, and manuscript writing and revision; AW: histological analysis, manuscript writing and revision, data analysis; CD and FW: surgery assistance, data analysis, and critical manuscript revision and writing; PH and HR: micro CT,

draft writing and revision; HT: data interpretation, discussion, biomechanical analysis, critical manuscript revision and writing; ER and MG: manuscript writing and revision, generation of sEVs; AT: funding, data interpretation, manuscript writing, and revisions. All authors have read and agreed to the published version of the manuscript.

Funding

The authors disclose receipt of the following financial or material support for the research: Lorenz Böhler Gesellschaft (grant number 1–21), AO Trauma—DACH Promotion of Young Talent, and Land Salzburg/IWB/EFRE 2014–2020 (Project #P1812596; “EV-TT”).

Data availability

All data analyzed during this study are included in this publication. The datasets during and/or analyzed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

All animal experiments and conducted procedures were in accordance with the Austrian law on animal experimentation and approved by the Austrian regulatory authorities.

Consent for publication

All authors have approved the final version of the manuscript.

Competing interests

The authors declare no competing interests. (1) Title of the approved project: “Regeneration of a metaphyseal defect in osteoporotic rats by implantation of exosomal vesicles”; (2) Name of the institutional approval committee: Federal Ministry of Education, Science and Research – V/3b (Animal testing and genetic engineering); (3) Approval Number: 2020–0.547.757; (4) Date of approval: 24.09.2020 The collection of human umbilical cord for isolation of mesenchyma stromal cells and enrichment of extracellular vesicles has been approved by the Ethics Commission for the State of Salzburg and informed consent was obtained from all donors (1). Title of the approved project: “Characterization of somatic cells and stem cells from human umbilical cord tissue”; (2) Name of the institutional approval committee: Ethics Commission for the State of Salzburg; (3) Approval Number: 415-E/1547/2-2012; (4) Date of approval: 05.11.2012.

Received: 3 November 2023 / Accepted: 7 May 2024

Published online: 20 May 2024

References

1. Sözen T, Özçişik L, Başaran N. An overview and management of osteoporosis. *Eur J Rheumatol*. 2017;4(1):46–56.
2. NIH Consensus Development Panel on Osteoporosis Prevention Da. Osteoporosis prevention, diagnosis, and therapy. *JAMA*. 2001;285(6):785–95.
3. Brown JP. Long-term treatment of postmenopausal osteoporosis. *Endocrinol Metab (Seoul)*. 2021;36(3):544–52.
4. Keller J, Catala-Lehnen P, Huebner AK, Jeschke A, Heckt T, Lueth A, et al. Calcitonin controls bone formation by inhibiting the release of sphingosine 1-phosphate from osteoclasts. *Nat Commun*. 2014;5:5215.
5. Wong RMY, Choy MHV, Li MCM, Leung KS, K-H Chow S, Cheung WH, et al. A systematic review of current osteoporotic metaphyseal fracture animal models. *Bone Joint Res*. 2018;7(1):6–11.
6. Liebig BE, Kisiday JD, Bahney CS, Ehrhart NP, Goodrich LR. The platelet-rich plasma and mesenchymal stem cell milieu: a review of therapeutic effects on bone healing. *J Orthop Res*. 2020;38(12):2539–50.
7. Marolt Presen D, Traweger A, Gimona M, Redl H. Mesenchymal stromal cell-based bone regeneration therapies: from cell transplantation and tissue Engineering to Therapeutic Secretomes and Extracellular vesicles. *Front Bioeng Biotechnol*. 2019;7:352.
8. Bowles-Welch AC, Jimenez AC, Stevens HY, Frey Rubio DA, Kippner LE, Yeago C, et al. Mesenchymal stromal cells for bone trauma, defects, and disease: considerations for manufacturing, clinical translation, and effective treatments. *Bone Rep*. 2023;18:101656.

9. Siegel G, Kluba T, Hermanutz-Klein U, Bieback K, Northoff H, Schafer R. Phenotype, donor age and gender affect function of human bone marrow-derived mesenchymal stromal cells. *BMC Med.* 2013;11:146.
10. Zeng ZL, Yuan Q, Zu X, Liu J. Insights into the role of Mitochondria in Vascular Calcification. *Front Cardiovasc Med.* 2022;9:879752.
11. Bruno S, Grange C, Deregibus MC, Calogero RA, Saviozzi S, Collino F, et al. Mesenchymal stem cell-derived microvesicles protect against acute tubular injury. *J Am Soc Nephrol.* 2009;20(5):1053–67.
12. Teo KYW, Tan R, Wong KL, Hey DHW, Hui JHP, Toh WS. Small extracellular vesicles from mesenchymal stromal cells: the next therapeutic paradigm for musculoskeletal disorders. *Cytotherapy.* 2023;25(8):837–46.
13. Zeng ZL, Xie H. Mesenchymal stem cell-derived extracellular vesicles: a possible therapeutic strategy for orthopaedic diseases: a narrative review. *Biomater Transl.* 2022;3(3):175–87.
14. Ebrahim N, Mostafa O, El Dosoky RE, Ahmed IA, Saad AS, Mostafa A, et al. Human mesenchymal stem cell-derived extracellular vesicles/estrogen combined therapy safely ameliorates experimentally induced intrauterine adhesions in a female rat model. *Stem Cell Res Ther.* 2018;9(1):175.
15. Sakou T. Bone morphogenetic proteins: from basic studies to clinical approaches. *Bone.* 1998;22(6):591–603.
16. McKay WF, Peckham SM, Badura JM. A comprehensive clinical review of recombinant human bone morphogenetic protein-2 (INFUSE bone graft). *Int Orthop.* 2007;31(6):729–34.
17. Deluca A, Wagner A, Faustini B, Weissenbacher N, Deininger C, Wichlas F et al. Development of a Metaphyseal Non-union Model in the osteoporotic rat femur. *Bioeng (Basel).* 2023;10(3).
18. Reinisch A, Strunk D. Isolation and animal serum free expansion of human umbilical cord derived mesenchymal stromal cells (MSCs) and endothelial colony forming progenitor cells (ECFCs). *J Visualized Experiments: JoVE.* 2009(32).
19. Romeis B. *Mikroskopische Technik von Mulisch, M., Welsch, U.* 18 ed: Springer: Heidelberg; 2010. p. 551.
20. Schindelin J, Arganda-Carreras I, Frise E, Kaynig V, Longair M, Pietzsch T, et al. Fiji: an open-source platform for biological-image analysis. *Nat Methods.* 2012;9(7):676–82.
21. Sarban S, Senkoylu A, Isikan UE, Korkusuz P, Korkusuz F. Can rhBMP-2 containing collagen sponges enhance bone repair in ovariectomized rats? A preliminary study. *Clin Orthop Relat Res.* 2009;467(12):3113–20.
22. Alt V, Thormann U, Ray S, Zahner D, Durselen L, Lips K, et al. A new metaphyseal bone defect model in osteoporotic rats to study biomaterials for the enhancement of bone healing in osteoporotic fractures. *Acta Biomater.* 2013;9(6):7035–42.
23. Kherad M, Mellström D, Rosengren BE, Hasserius R, Nilsson J, Redlund-Johnell I, et al. The number and characteristics of prevalent vertebral fractures in elderly men are associated with low bone mass and osteoporosis. *Bone Joint J.* 2015;97–B(8):1106–10.
24. Huang K, Wu G, Zou J, Peng S. Combination therapy with BMP-2 and psoralen enhances fracture healing in ovariectomized mice. *Exp Ther Med.* 2018;16(3):1655–62.
25. Park SB, Park SH, Kim NH, Chung CK. BMP-2 induced early bone formation in spine fusion using rat ovariectomy osteoporosis model. *Spine J.* 2013;13(10):1273–80.
26. Buzas EI. Opportunities and challenges in studying the extracellular vesicle corona. *Nat Cell Biol.* 2022;24(9):1322–5.
27. Kowal J, Arras G, Colombo M, Jouve M, Morath JP, Primdahl-Bengtson B, et al. Proteomic comparison defines novel markers to characterize heterogeneous populations of extracellular vesicle subtypes. *Proc Natl Acad Sci U S A.* 2016;113(8):E968–77.
28. Toth EA, Turiak L, Visnovitz T, Cserep C, Mazlo A, Sodar BW, et al. Formation of a protein corona on the surface of extracellular vesicles in blood plasma. *J Extracell Vesicles.* 2021;10(11):e12140.
29. Reddy SK, Ballal AR, Shailaja S, Seetharam RN, Raghu CH, Sankhe R, et al. Small extracellular vesicle-loaded bevacizumab reduces the frequency of intravitreal injection required for diabetic retinopathy. *Theranostics.* 2023;13(7):2241–55.
30. Buzas EI, György B, Nagy G, Falus A, Gay S. Emerging role of extracellular vesicles in inflammatory diseases. *Nat Rev Rheumatol.* 2014;10(6):356–64.
31. Jenner F, Wagner A, Gerner I, Ludewig E, Trujanovic R, Rohde E, et al. Evaluation of the potential of umbilical cord mesenchymal stromal cell-derived small Extracellular vesicles to improve Rotator Cuff Healing: a pilot ovine study. *Am J Sports Med.* 2023;51(2):331–42.
32. Romanelli P, Bieler L, Heimel P, Skokic S, Jakubecova D, Kreutzer C, et al. Enhancing functional recovery through Intralesional Application of Extracellular vesicles in a rat model of traumatic spinal cord Injury. *Front Cell Neurosci.* 2021;15:795008.
33. Escrevente C, Keller S, Altevogt P, Costa J. Interaction and uptake of exosomes by ovarian cancer cells. *BMC Cancer.* 2011;11:108.
34. Janas AM, Sapoń K, Janas T, Stowell MH. Exosomes and other extracellular vesicles in neural cells and neurodegenerative diseases. *Biochim Biophys Acta.* 2016;1858(6):1139–51.
35. Morelli AE, Larregina AT, Shufesky WJ, Sullivan ML, Stolz DB, Papworth GD, et al. Endocytosis, intracellular sorting, and processing of exosomes by dendritic cells. *Blood.* 2004;104(10):3257–66.
36. Xu J, Wang Y, Hsu CY, Gao Y, Meyers CA, Chang L et al. Human perivascular stem cell-derived extracellular vesicles mediate bone repair. *Elife.* 2019;8.
37. Lai CP, Mardini O, Ericsson M, Prabhakar S, Maguire C, Chen JW, et al. Dynamic biodistribution of extracellular vesicles in vivo using a multimodal imaging reporter. *ACS Nano.* 2014;8(1):483–94.
38. Xu CM, Sabe SA, Brinck-Teixeira R, Sabra M, Sellke FW, Abid MR. Visualization of cardiac uptake of bone marrow mesenchymal stem cell-derived extracellular vesicles after intramyocardial or intravenous injection in murine myocardial infarction. *Physiol Rep.* 2023;11(6):e15568.
39. Simonsen JB. Pitfalls associated with lipophilic fluorophore staining of extracellular vesicles for uptake studies. *J Extracell Vesicles.* 2019;8(1):1582237.
40. Takov K, Yellon DM, Davidson SM. Confounding factors in vesicle uptake studies using fluorescent lipophilic membrane dyes. *J Extracell Vesicles.* 2017;6(1):1388731.
41. Russo E, Alberti G, Corrao S, Borlongan CV, Miceli V, Conaldi PG et al. The truth is out there: biological features and clinical indications of Extracellular vesicles from human perinatal stem cells. *Cells.* 2023;12(19).
42. Warnecke A, Prenzler N, Harre J, Kohl U, Gartner L, Lenarz T, et al. First-in-human intracochlear application of human stromal cell-derived extracellular vesicles. *J Extracell Vesicles.* 2021;10(8):e12094.
43. Garrison KR, Shemilt I, Donell S, Ryder JJ, Mugford M, Harvey I, et al. Bone morphogenetic protein (BMP) for fracture healing in adults. *Cochrane Database Syst Rev.* 2010;2010(6):CD006950.
44. U.S. Food and Drug Administration c-a. InFuse TM Bone Graft/LT-CAGETM lumbar tapered fusion device-P000058. 2002; 2002.
45. Bess S, Line BG, Lafage V, Schwab F, Shaffrey CI, Hart RA, et al. Does recombinant human bone morphogenetic protein-2 use in adult spinal deformity increase complications and are complications associated with location of rhBMP-2 use? A prospective, multicenter study of 279 consecutive patients. *Spine (Phila Pa 1976).* 2014;39(3):233–42.
46. Simmonds MC, Brown JV, Heirs MK, Higgins JP, Mannion RJ, Rodgers MA, et al. Safety and effectiveness of recombinant human bone morphogenetic protein-2 for spinal fusion: a meta-analysis of individual-participant data. *Ann Intern Med.* 2013;158(12):877–89.
47. Faundez A, Tournier C, Garcia M, Aunoble S, Le Huec JC. Bone morphogenetic protein use in spine surgery—complications and outcomes: a systematic review. *Int Orthop.* 2016;40(6):1309–19.
48. Meijering EH, Niessen WJ, Viergever MA. Quantitative evaluation of convolution-based methods for medical image interpolation. *Med Image Anal.* 2001;5(2):111–26.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.